

30357_17_lecture_9_12

z direction

 $\rho\left(\frac{\partial v_z}{\partial t} + v_x \frac{\partial v_z}{\partial t} + v_y \frac{\partial v_z}{\partial y} + v_z \frac{\partial v_z}{\partial z}\right) = \frac{\partial p}{\partial z} + \mu \left[\frac{\partial^2 v_z}{\partial x^2} + \frac{\partial^2 v_z}{\partial y^2} + \frac{\partial^2 v_z}{\partial z^2}\right] + \rho g_z$

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A subtle and perhaps confusing argument will now be given!

We conclude that V_x does not change in x.

We conclude that $\frac{\partial P}{\partial x}$ does not change with y

Hence, the only way for these terms to be always equal is if they are equal to a constant.

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The mechanism of exercise-induced asthma is . . .

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Figure 1. Airway diameters (mm) drawn against airway generations. (Adapted with permission from Ref. 6.)

MECHANISMS OF REMODELLING

perhaps best illustrated by irritant-induced asthma. Certain characteristic changes, such as growth of ASM, seem likely to contribute to airways hyperresponsiveness (AHR), but the consequences of other changes, such as subepithelial fibrosis, are not so intuitively obvious. Even the link between growth of ASM and AHR is deduced largely on the basis of modelling studies. One of the major challenges facing the field is to devise strategies that link structure and function directly. For

Airway smooth muscle (remodeling)

Suppose we want to consider the flow in a trachea.

The geometry is a cylinder.

We need the Navier-Stokes equations in cylindrical coordinates.

Cylindrical coordinates

r direction

$$
\rho \left(\frac{\partial Y}{\partial r} + \gamma \frac{\partial Y}{\partial r} + \frac{\partial \theta}{r} \frac{\partial Y}{\partial \theta} - \frac{\partial \theta}{r} + v_z \frac{\partial Y}{\partial \theta} \right) = \frac{\partial \rho}{\partial r} + \mu \left[\frac{\partial}{\partial r} \left(\frac{1}{r} \frac{\partial (\rho \phi)}{\partial r} \right) + \frac{1}{r^2} \frac{\partial Y}{\partial \theta^2} - \frac{2}{r^2} \frac{\partial \phi}{\partial \theta} + \frac{\partial^2 Y}{\partial z^2} \right] + \rho \phi \tag{3.3.27a}
$$

 θ direction

$$
\rho \left(\frac{\partial \mathcal{L}}{\partial r} + v_r \frac{\partial \mathcal{L}}{\partial r} + \frac{\partial \mathcal{L}}{\partial r} \frac{\partial \mathcal{L}}{\partial r} + \frac{\partial \mathcal{L}}{\partial \theta} + v_z \frac{\partial \mathcal{L}}{\partial \tau} \right) = -\frac{1}{r} \frac{\partial \rho}{\partial \theta} + \mu \left[\frac{\partial}{\partial r} \left(\frac{1}{r} \frac{\partial (r \mathbf{v} \mathbf{s})}{\partial r} \right) + \frac{1}{r^2} \frac{\partial^2 \mathcal{L}}{\partial \theta^2} + \frac{2}{r^2} \frac{\partial v_r}{\partial \theta} + \frac{\partial^2 \mathcal{L}}{\partial \tau^2} \right] + \rho \mathbf{v} \tag{3.3.27b}
$$

$$
\frac{\rho(\frac{N_{\epsilon}}{jk} + \gamma \frac{N_{\epsilon}}{jk} + \gamma \frac{N_{\epsilon}}{jk} + \gamma \frac{N_{\epsilon}}{jk}) - \frac{2p}{\sqrt{K}} \cdot \frac{1}{\mu[\frac{1}{r}, \frac{1}{m}(\frac{1}{r}, \frac{1}{m})} + \frac{1}{r} \frac{3\sqrt{K}}{jk} + \frac{3\sqrt{K}}{jk}] - \rho_{\epsilon}}{j} - \frac{1}{\mu} \
$$

NOW CONSIDER CASE 1: FLOW BY GRAVITY $0 = \frac{M}{\pi} \frac{2}{51} \times \frac{212}{51} + 582$ $\frac{M}{\lambda}$ and $\frac{dy}{d\lambda} = -992$ $\frac{d}{dt}$ $\wedge \frac{d}{dt} = \frac{-g}{dt}$ γz $d(\Lambda \frac{d\Uparrow e}{d\Lambda}) = -\frac{e}{\Lambda}g_{z}\Lambda d\Lambda$ $1\frac{dV}{d\lambda} = -\frac{Q}{\mu} \frac{d^2}{d^2} + C_1$ $dV_z = (8 + 92 + 5 + 5)dx$ $V_{2} = -\frac{\rho}{\mu} - \frac{\rho}{4} + C_{1}$ $ln A + C_{2}$

Boundary conditions:

- 1. Fluid sticks to solid surfaces $V_{\mathbf{X}}(\partial)=\partial$
- 2. Fluid sticks to another immiscible fluid $V_x^{\pm}(h) = V_x^{\pm}(h)$
- 3. The shear stress is continuous across the fluid-fluid interface

4. For liquid flowing next to quiescent air, the stress can be considered approximately 0.

 $FAU-1N6$